

Synthesis of Mammographic Images Based on the Fractional Brownian Motion

Ines Slim Sahli^{1,*}, Hanen Bettaieb¹, Asma Ben Abdallah¹, Imen Bhouiri², Mohamed Hedi Bedoui¹

¹Faculty of Medecine of Monastir, University of Monastir, Monastir, Tunisia

²Research Unit Wavelet and Multifractal, Faculty of Science of Monastir, University of Monastir, Monastir, Tunisia

Email address:

slim_ines5@yahoo.com (I. S. Sahli), hanen.bettaiebl@gmail.com (H. Bettaieb), assoumaba@yahoo.com (A. B. Abdallah), bhouiri.imen@gmail.com (I. Bhouiri), hedi.bedoui2015@gmail.com (M. H. Bedoui)

*Corresponding author

To cite this article:

Ines Slim Sahli, Hanen Bettaieb, Asma Ben Abdallah, Imen Bhouiri, Mohamed Hedi Bedoui. Synthesis of Mammographic Images Based on the Fractional Brownian Motion. *International Journal of Medical Imaging*. Vol. 6, No. 1, 2018, pp. 1-8. doi: 10.11648/j.ijmi.20180601.11

Received: January 25, 2018; **Accepted:** February 5, 2018; **Published:** February 27, 2018

Abstract: This paper presents a new approach for synthesizing breast tissue images based on a random fractal process, the fractional Brownian motion (fBm). This work deals with modeling Regions of Interest (ROIs) of mammographic images. Diverse synthetic ROIs were generated: healthy ones and others with microcalcifications according to fatty and dense tissue. Microcalcifications were injected in several dispositions in order to model benign and malignant cases. The aim of this study resides in two points: (1) the generation of synthetic images of mammograms for researchers and radiologists in order to test their tools and orient the choice of their parameters to enhance the diagnostic accuracy; and (2) to compare two microcalcification segmentation approaches: 'Sq-Sq' approach based on multifractal analysis and the 'MM' approach based on Mathematical Morphology. In fact, the results proved that the 'Sq-Sq' method can detect microcalcifications with different arrangements for any type of tissue and were evaluated using a qualitative test by an expert and a quantitative one based on the Area Overlap Measure (AOM) and the Dice coefficient. The 'Sq-Sq' approach yield a mean of 0.8 ± 0.06 for AOM and 0.8446 for Dice coefficient for all segmented images.

Keywords: Synthetic Images, fBm, Mammography, Microcalcifications, Segmentation

1. Introduction

Breast cancer is among the leading cause of death for women [1]. The first signs of breast cancer are microcalcifications, which are small calcium deposits in the breast tissue. Mammography is the most widely used for their detection [2, 3]. Clinical studies have confirmed that the survival rate is considerably increased if anomalies are detected at early stages [4]. Their detection is a hard task in medical imaging due to several factors such as their irregular form and their small size which varies from 0.1 to 1 mm [4, 5]. They are approximately nodular, but with irregular shape arrangements. Furthermore, microcalcifications frequently appear with a local contrast. This contrast is often low and varies according to the breast tissue type. Therefore, these clusters should be detected to establish a correct diagnosis.

There are several types of breast tissue [6], but from the perspective of x-ray attenuation it can be modeled as consisting solely of two types of tissues: fatty and dense tissues, which vary according to their breast density [6]. They are also characterized by several physical properties and various distributions of the grayscale level. Such diversity produces different complexity degrees when detecting microcalcification in the mammogram, especially in the case of dense tissue. For these reasons, microcalcification detection is not easy even for trained radiologists, and they may go undetected. Therefore, the clinical interpretation of mammograms remains rather subjective and diagnosis is often debatable [7]. This has encouraged us to build synthetic ROIs of mammograms.

The variety of background tissue structure, the irregular

shapes and the various arrangements of microcalcifications led to the use of a random fractal process: the fractional Brownian motion (fBm). This process has three main properties that closely resemble the natural texture of mammographic images: fractal dimension, scale invariance and self-similarity [8, 9], which seems to be appropriate to model this type of images [8].

The fBm model proposed by Mandelbrot, B.B et al [10] is used to describe natural fractal phenomenon. Moreover, it was applied [11-14] to generate synthetic images and compare the accuracy of several fractal methods.

In this work, the fBm was investigated to synthesize ROIs of mammographic images. Four groups of synthetic images were generated: healthy group and with microcalcifications group for the both type of tissue (fatty and dense). These images can be helpful for radiologists to test their tools and guide the choice of their parameters in order to enhance the diagnostic accuracy of breast cancer at an early stage. Also, they help researchers rate the accuracy of their approaches in detecting anomalies. Besides, these mammogram models can be used to compare microcalcification segmentation approaches.

In the literature, several approaches were proposed to segment microcalcifications [15-18] such as active contours [16, 19], curvelet moments [20], wavelet analysis [21-23], fractal analysis [24-26], multifractal analysis [27, 28] and morphological filters [29-32] in order to reduce human subjectivity in diagnosis.

In this paper, the synthetic images were applied on two algorithms of microcalcification segmentation the new approach ‘Sq-Sq’ [28] and the reference approach ‘MM’ [29] to compare them. The ‘Sq-Sq’ method used a novel multifractal spectrum measure based on the q-structure function [33], which is a well-known tool for analyzing an object’s irregularity. The ‘MM’ approach [29] is based on the Mathematical Morphology and the Otsu algorithm [34]. The evaluation of these approaches was checked using the Area Overlap Measure (AOM) [35] and the Dice coefficient [36].

This paper is organized as follows: in section 2, the fBm characteristics are explained and the generation of synthetic images of mammograms is detailed. An overview of the segmentation methods applied on the synthetic images of mammograms is presented in section 3. The results are shown and discussed in sections 4 and 5. Finally, a conclusion that highlights our contribution and exposes our perspectives was presented.

2. Breast Tissue Modeling

Some works were interested also in generating synthetic images of mammograms as [37] and more recently [38] which are based on the fractional Brownian motion and presented good results. Developing synthetic images for breast tissue with microcalcifications remains complex as well as

interesting because of the variety of background tissues and irregular shapes of microcalcifications. As previously mentioned, the fBm can be adequate to simulate ROIs of mammograms [8]. In this section, some basic notions about the fBm that justify the selected choice were presented. In this work, the fBm process was used to create different classes of tissue: class of healthy and class of patients (i.e. with microcalcifications) for the both type of tissue (fatty and dense).

2.1. Fractional Brownian Motion (fBm)

fBm is a generalization of classical Brownian motion. It is a stochastic fractal process with long-range dependence and self-similar behaviors [10]. The Hurst coefficient H ($0 < H < 1$) is the unique parameter of interest of fBm process. In fact, it describes the roughness of the resultant motion: the higher is H , the smoother is the motion.

The FBm spectral representation $B_H(t)$ is given by [39]:

$$B_H(t) = \frac{1}{2\pi} \int_{-\infty}^{+\infty} \frac{1}{(i\omega)^{H+\frac{1}{2}}} (e^{it\omega} - 1) dB(\omega) \quad (1)$$

It is a Gaussian, continuous, centered and non-stationary second-order process which starts at zero ($B_H(0) = 0$) and has the following covariance function:

$$E[B_H(t)B_H(s)] = \frac{1}{2} (|t|^{2H} + |s|^{2H} + |t-s|^{2H}) \quad (2)$$

To model background tissue of mammograms which are self-similar object [8], the Stein’s method [40] was used. It is a fast and exact approach for simulating fractional Brownian surfaces [40].

2.2. Healthy Synthetic ROIs

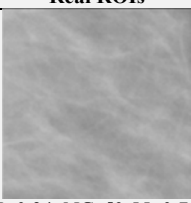
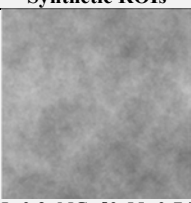
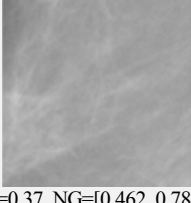
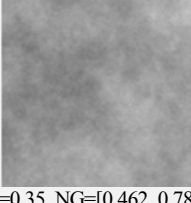
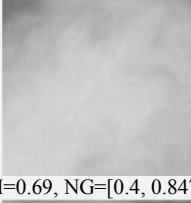
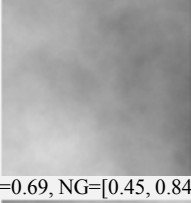
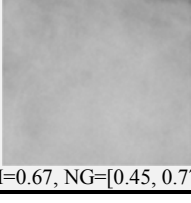
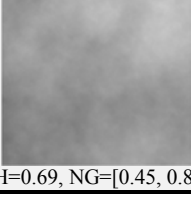
Kestener, P., et al. [41] proved that normal regions in digitized mammograms are characterized by the Hurst coefficient $H=0.3 \pm 0.1$ in fatty tissue whereas dense region have $H=0.65 \pm 0.1$.

Based on the study [41], generation of synthetic mammographic ROIs is proposed using the values of H cited above. The background tissues (dense and fatty) were generated based on the Stein method [40]. These ones are simulated with the corresponding Hurst coefficient H and the grayscale variation of ROIs selected from Mini-MIAS [42]. The Hurst coefficient H of each selected ROI was estimated with the quadratic variation method [43].

The synthetic ROIs are sized of (128×128) pixels with resolution of 0.2 mm. The gray level ‘NG’ of the pixel is normalized between 0 and 1. Table 1 shows some examples of healthy real ROIs of Mini-MIAS and the corresponding models.

As shown in Table 1, these synthetic images (third colon) accurately modeled real mammographic backgrounds (second colon). H is the Hurst coefficient and NG is the interval of the normalized gray level.

Table 1. Examples of background ROIs and the corresponding models.

Type of tissue	Real ROIs	Synthetic ROIs
Fatty		
	H=0.34, NG=[0.55, 0.74]	H=0.3, NG=[0.55, 0.74]
Dense		
	H=0.37, NG=[0.462, 0.784]	H=0.35, NG=[0.462, 0.784]
		
	H=0.69, NG=[0.4, 0.847]	H=0.69, NG=[0.45, 0.847]
		
	H=0.67, NG=[0.45, 0.77]	H=0.69, NG=[0.45, 0.8]

For the rest of this work, the variability of the gray level of the background tissue was controlled according to ROIs selected randomly from healthy mammograms of Mini-MIAS dataset [42] which allow discrimination between fatty and dense tissue. After analyzing 100 healthy ROIs for each type of tissue, it was concluded that the mean of grayscale level of fatty tissue was in the interval [115, 200] and that dense tissue was characterized by grayscale level usually in the interval [160, 222].

Although scanned and digital mammograms were generally obtained in 12-bit and usually stored as 16-bit images, there were no unfavorable effects when reduced to 8-bit. For faster computational analysis [19, 27, 44, 45] or reduction of storage demands [46], the synthetic ROIs were generated as an 8-bit grayscale image.

2.3. Synthetic ROIs with Microcalcifications

Microcalcifications have different sizes and irregular dispositions [47], which can differentiate between benignity and malignancy. If they are round, oval, or slightly lobular, the anomaly is probably benign. If the microcalcifications are arranged on an irregular or tubular shape, then they are suggestive of malignancy. Microcalcifications are small light details and are highly invisible within the background tissue.

According to radiologists [47], microcalcifications have usually circular forms. For this reason, microcalcifications are modeled as small circles with a radius equal to 1 pixel

obtained from the same background tissue but slightly clearer especially in the case of dense tissue. So, the visibility of anomalies is more difficult with dense cases. Each healthy synthetic ROI is injected with these ones to obtain synthetic ROIs with microcalcifications. It should be noted that synthetic microcalcifications are arranged in several dispositions to obtain malign and benign cases. Malignant cases are generally characterized by almost linear arrangement of microcalcifications [41]. However, benign cases have approximately a circular disposition [47].

Figure 1. presents a model of the whole part of mammogram sized (512×512) which can contain anomalies. As it is clear, it is difficult to detect microcalcifications by naked eyes. To simplify the study, ROIs sized (128×128) were modeled.

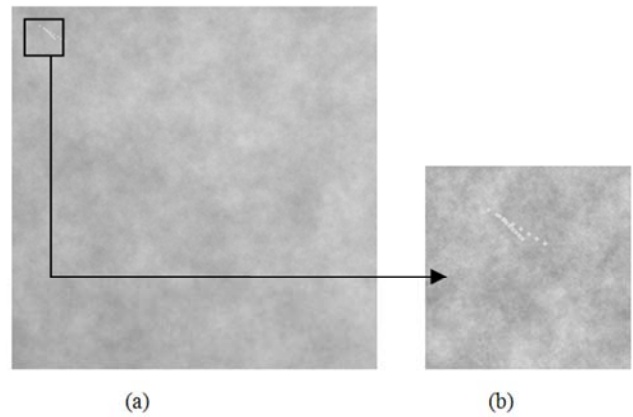
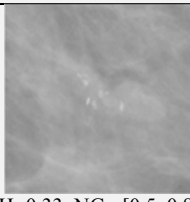
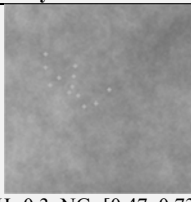
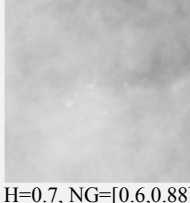
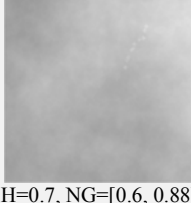
**Figure 1.** (a) Example of synthetic model for a whole part of fatty mammogram (512×512) that contains microcalcifications, (b) a selected ROI from (a) (black square).

Table 2 shows two real ROIs and their corresponding synthetic images which are generated with the same parameters of real ROIs (H coefficient and grayscale variability).





Table 2. Examples of real ROIs with microcalcifications and the corresponding synthetic images.

Type of tissue	Real ROIs	synthetic ROIs
Fatty		
	H=0.33, NG=[0.5, 0.8]	H=0.3, NG=[0.47, 0.73]
Dense		
	H=0.7, NG=[0.6, 0.88]	H=0.7, NG=[0.6, 0.88]

As shown, synthetic images seem 'like' real ones. In addition, they have the same mathematical characteristics.

According to radiologists, the dense tissue with the brightest grayscale is the hard case. As already mentioned, it is possible to generate an infinite number of images since a random process, the fBm, was used. Table 3 shows other synthetic images of benign and malignant cases for fatty and dense tissue. Synthetic microcalcifications are small circles (radius equal to 1 pixel) selected from the same tissue of the background but with pixel intensity slightly clearer.

Table 3. Synthetic ROIs with microcalcifications for fatty and dense tissue: (a), (b) present benign cases; (c), (d) show malignant cases.

Type of tissue	Benign cases	Malignant cases
Fatty	 H=0.35, NG = [0.5, 0.7]	 H=0.4, NG= [0.5,0.78]
Dense	 H=0.7, NG=[0.65, 0.9]	 H=0.7, NG= [0.6, 0.88]

3. Microcalcification Segmentation Methods Applied on the Synthetic Images

In the present work, the generated synthetic images were used to evaluate and compare the ‘Sq-Sq’ approach [28] based on the multifractal analysis and another reference work based on the morphological operators; the ‘MM’ [29] approach. This assists to orient the choice of their initial parameters in order to ameliorate their results in future works.

3.1. Approach based on Multifractal Analysis

In a previous work [28], a segmentation approach based on the combination of multifractal analysis with the k-means algorithm followed by morphological operators, noted ‘Sq-Sq’, was proposed. This method was applied on real mammograms from the reference database MiniMias [42]. This segmentation approach consists mainly of four steps. After the construction of ‘ α _image’ and the ‘ $f(\alpha)$ _image’ based respectively on multifractal and fractal analysis, the k-means algorithm followed by morphological operators (closing and opening) was applied to the ‘ $f(\alpha)$ _image’ to segment the anomalies. The two first steps enhance the visualization of microcalcifications and facilitate their extraction. Figure 2. shows the flowchart of the ‘Sq-Sq’ approach.

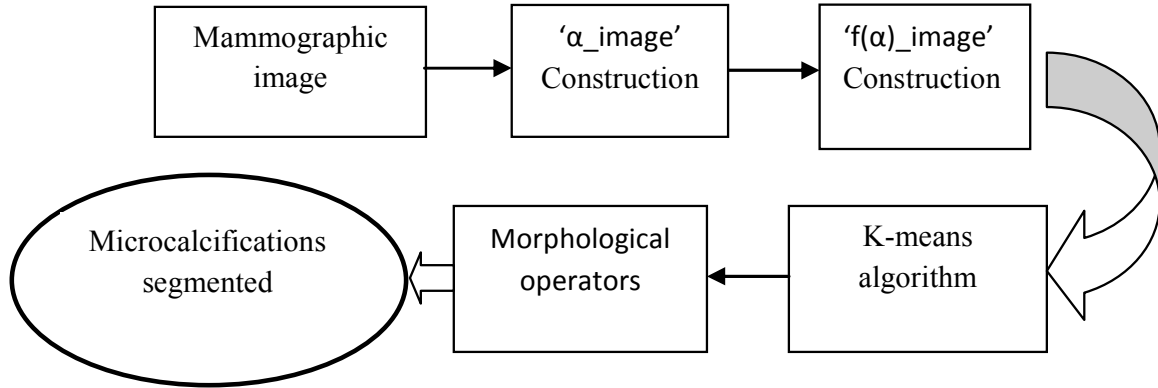


Figure 2. The flowchart of the ‘Sq-Sq’ segmentation approach.

3.2. Approach based on Mathematical Morphology ‘MM’

The microcalcification segmentation approach ‘MM’ [29] was based on morphological operators and the Otsu’s method. The authors of [29] applied a pre-processing with top-hat operators which enhance the contrast and reduce the background noise. In [29], the microcalcifications were selected automatically based on the Otsu’s method that finds the more adequate grayscale level threshold to segment the image.

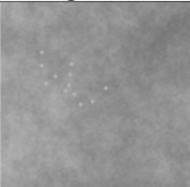
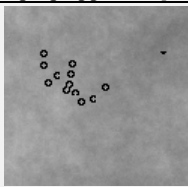
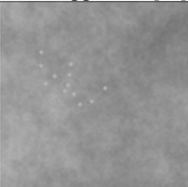
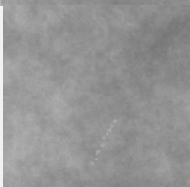
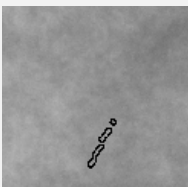
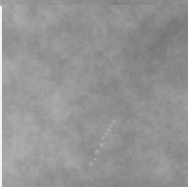



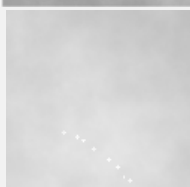


4. Results

The used database of generated synthetic images contains

300 synthetic images with 100 images showing healthy tissue (dense and fatty) and 200 synthetic images with microcalcifications (benign and malignant). To the best of the knowledge of authors; an infinite number of models can be generated since a stochastic process was used.

The segmentation methods [28, 29] were applied to the simulated images in order to compare them. Table 4 shows the segmentation result of some synthetic images for the two types of tissue (fatty and dense). The original image and the original image with superimposed contour lines around segmented microcalcifications by each approach are illustrated in Table 4.

Table 4. Segmentation of synthetic images sized (128×128) pixels.

		Original ROI	'Sq-Sq' approach [28]	'MM' approach [29]
Fatty	Benign			
	Malignant			
Dense	Benign			
	Malignant			

According to radiologists' experience, the 'Sq-Sq' [28] approach provides good segmentation results and the 'MM' method [29] succeeded in segmenting microcalcifications in only two dense cases. Consequently, this method is able to detect microcalcifications with very small size only in smooth backgrounds: high Hurst coefficient and high gray level. Also, these incomplete results of segmentation may be due to the size of images (see Table 5). Since, in all Marcelo Duarte et al works [19, 29], the authors used ROIs with small size 41×41 pixels, hence other synthetic images were generated (see Table5) to further check the features of the segmentation approaches 'Sq-Sq' [28] and 'MM' [29]. As the exact size 41×41pixels can't be obtained with the Stein method [40] (the image size can only be $2^{(n-1)}$; n integer), these synthetic images are sized 32×32 pixels (n=6).

Note that M. Duarte et al [19] approach was not applied on the simulated images because it is based on Geodesic Active Contours (GAC) segmentation method which needs a seed point.

Furthermore, this method is sensitive to the choice of the last one. In other words, if a seed point is selected in different places on the image, results will be different.

So, it is important to try hard to put them near the centroid point of the lesion to segment.

As 'MM' method [29] was much more robust than GAC for segmenting microcalcifications [19]. Table 5 shows examples of models sized (32×32) pixels.

Table 5. Segmentation of synthetic images sized (32×32) pixels.

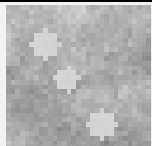
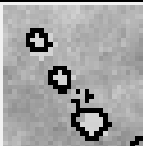
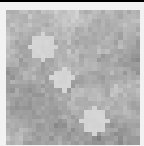
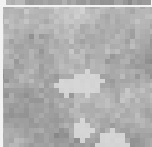

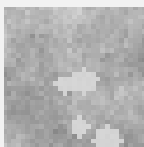


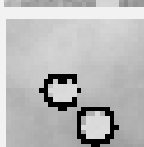
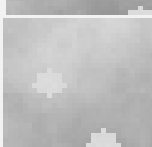

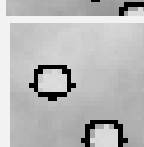


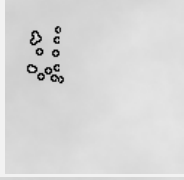

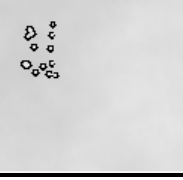

		Original ROI	'Sq-Sq' Approach [28]	'MM' Approach [29]
Fatty tissue				
				
Dense tissue				
				

Table 6 presents some examples of dense synthetic images with smooth background which will be applied to the 'Sq-Sq' [28] and the 'MM' [29] approaches.

According to Table 5 and Table 6, the 'MM' approach [29] can segment microcalcifications only in smooth background no matter what the size is, whereas the 'Sq-Sq' approach [28] can extract anomalies whatever the type of tissue is. Good results

are obtained for sized (128×128) pixels models but there are incomplete results for smaller dense models sized (32×32). This can be explained by the Sq equation (i.e, equation (1) in [28]) which needs to use the grayscale of the neighbor pixels. The larger the image is the better the results are.

Table 6. Segmentation of dense models (benign and malignant cases).

	Benign cases	Malignant cases
Original Models		
'Sq-Sq' segmentation		
'MM' segmentation		

5. Statistical evaluation

Besides the qualitative evaluation, a quantitative evaluation of the two approaches [28, 29] based on the area overlap measure (AOM) [35] and Dice Similarity coefficient [36] was conducted. The 200 synthetic ROIs, with injected microcalcifications, were manually delineated (i.e., segmented) with GIMP 2.8 software. The sizes as well as the locations of microcalcification were known in advance. These images were considered as the ground truth for calculating the AOM and Dice coefficient.

5.1. Area Overlap Measure (AOM)

The AOM is expressed as:

$$AOM = \frac{\text{area}(G_Th \cap IM_Seg)}{\text{area}(G_Th \cup IM_Seg)} \quad (3)$$

In this equation, G_Th denotes the microcalcification manually delineated and IM_Seg represents the segmentation obtained using the proposed method. The symbol \cap denotes the intersection, i.e., the number of common pixels between G_Th and IM_Seg , and the symbol \cup represents the union of the G_Th and IM_Seg areas. So, if there is no overlap between the delineated microcalcification and the one from the proposed method, $AOM = 0$.

For a complete overlap, $AOM = 1$.

5.2. Dice Similarity Coefficient

Dice similarity coefficient measures the similitude between two sets G_Th and IM_Seg , the Dice coefficient is calculated

as in the following equation:

$$Dice_coeff = 2 \times \frac{\text{overlap area of } IM_Seg \text{ and } G_Th}{\text{total area of } IM_Seg \text{ and } G_Th} \quad (4)$$

Table 7 shows the statistical evaluation based on AOM measure and Dice coefficient of the 'Sq-Sq' approach [28] and the 'MM' approach [29].

Table 7. Statistical evaluation.

	'Sq-Sq' approach [28]	'MM' approach [29]
AOM	0.8±0.06	0.7±0.05
Dice	0.8446	0.5423

6. Discussion

The present work deals with ROIs of mammogram modeling based on the fBm process. Synthetic ROIs with microcalcifications and healthy ones were generated. Two types of tissues (fatty and dense) and the two types of severity (benign and malignant) were considered. The synthetic ROIs were modeled based on the Stein method [40]. The Hurst coefficients were chosen according to [41]; $H=0.3\pm0.1$ for fatty tissue and $H=0.65\pm0.1$ for dense tissue. The discrimination between tissues' types was controlled according to the grayscale deduced from the study of real cases, mammographic images of Mini-MIAS database [42]. In order to obtain synthetic ROIs similar to the real cases, a large number of models were generated randomly with different values of the Hurst coefficient H , diverse grayscale variations and several arrangements of microcalcifications.

Two referenced approaches of microcalcification segmentation: the 'Sq-Sq' [28] and the 'MM' [29] methods were applied on the developed synthetic images in order to compare them. The evaluation was carried out qualitatively according to the opinion of a skilled radiologist, as well as quantitatively based on two evaluation criteria: AOM and Dice coefficients. The results showed that the 'Sq-Sq' method was able to detect anomalies on synthetic ROIs sized (128×128) pixels independently of the tissue type. However, for models sized (32×32) pixels, the 'Sq-Sq' succeeded in extracting microcalcifications from only fatty models. This limit can be explained by the fact that the 'Sq-Sq' approach is based on calculating the difference between the pixel's grayscale.

The 'MM' method [29] yielded incomplete results for the segmentation of models sized (128×128) pixels especially for fatty tissue (small value of H : rough surface). The authors of [29] usually used ROIs sized (41×41) pixels, which urged us to construct another set of models sized (32×32) pixels, in order to check if the failed results were related to either the size or type of tissue. These results also showed incomplete segmentation of microcalcifications in rough surfaces (fatty tissue). The 'MM' approach [29] presented good results of segmentation in a smooth background (dense tissue) independently to the size. The 'Sq-Sq' approach yielded pertinent findings for large fatty and dense models. However, for models sized (32×32) pixels the 'Sq-Sq' succeeded only in

fatty models (low value of H). The 'Sq-Sq' is based on the calculation of the difference between grayscale neighbors' pixels, which can explain why segmentation failed in dense small models sized (32×32) pixels.

The 'Sq-Sq' approach yielded an average of 0.8 ± 0.06 for AOM measure and Dice coefficient of 0.8446. The 'Sq-Sq' method had a good performance regardless of the type of tissue and the severity's type. The latter depends on the size of the images. The 'MM' approach presented satisfactory results for images with a smooth background regardless of the size. It achieved an average of 0.7 ± 0.05 for AOM measure and Dice coefficient of 0.5423. However, the 'MM' approach could give pertinent segmentation only for models having smooth background i.e. high grayscale variability even for very small microcalcifications.

7. Conclusion and perspectives

In this work, a novel approach of synthetic images generation based on fBm process was proposed. The main objective was twofold: (1) to offer reference images for researchers and radiologists to test respectively the accuracy of their algorithms and the precision of their diagnostic tools; (2) to compare two microcalcification segmentation approaches: 'Sq-Sq' [28] and 'MM' [29], which helps to orient the choice of their parameters so as to obtain better results. Segmented images were evaluated in two ways: a qualitative and quantitative evaluation. Satisfactory segmentation was achieved by applying the 'Sq-Sq' method to the synthetic images. In fact, the 'Sq-Sq' approach gave good results for fatty and dense tissue. According to experts, the generated synthetic ROIs of mammographic images can help radiologists to test the precision of their diagnosis.

It can be concluded that the synthetic ROIs can be applied on several approaches of microcalcification segmentations to test their parameters and check if there are any gaps.

As perspectives, we suggest to generate a larger number of synthetic images and further diversify our examples by mainly varying the arrangement of the injected microcalcifications. This would allow us to study other synthetic images of mammograms especially for benign and malignant cases. We also propose modeling a whole mammogram with the various types of tissue.

References

- [1] Centers for Disease Control and Prevention, Cancer Among Women, 2015. Available from: <http://www.cdc.gov/cancer/dcpc/data/women.html> (accessed on 15-12-2017).
- [2] Elmore, Joann G. "Breast cancer screening: balancing evidence with culture, politics, money, and media." *Breast Cancer Screening*. 2016. 1-27.
- [3] Pretorius, E. Scott, and Jeffrey A. Solomon. *Radiology Secrets Plus E-Book*. Elsevier Health Sciences, 2010.
- [4] L. Tabar, S. Duffy, L. Burhenne, New Swedish breast cancer detection results for women aged 40–49, *Cancer* 72 (suppl.) (1993)1437. [http://dx.doi.org/10.1002/1097-0142\(19930815\)](http://dx.doi.org/10.1002/1097-0142(19930815)).
- [5] J. Bronzino (Ed.), *Biomedical Engineering Handbook*, CRC Press, Boca Raton, FL, 1995.
- [6] American College of Radiology. *ACR BI-RADS – Mammographie* (2e édition française basée sur la 4e édition américaine). In: *ACR Breast Imaging Reporting and Data System, Breast Imaging Atlas*, 2003.
- [7] Soares, Filipe, et al. "3D lacunarity in multifractal analysis of breast tumor lesions in dynamic contrast-enhanced magnetic resonance imaging." *IEEE Transactions on Image Processing* 22.11 (2013): 4422-4435.
- [8] McGarry, G., & Deriche, M. (1997, December). Modelling mammographic images using fractional Brownian motion. In *TENCON'97. IEEE Region 10 Annual Conference. Speech and Image Technologies for Computing and Telecommunications.*, Proceedings of IEEE (Vol. 1, pp. 299-302). IEEE.
- [9] Li, H., Giger, M. L., Olopade, O. I., & Chinander, M. R. (2008). Power spectral analysis of mammographic parenchymal patterns for breast cancer risk assessment. *Journal of digital imaging*, 21(2), 145-152. <http://dx.doi.org/10.1007/s10278-007-9093-9>
- [10] Mandelbrot, B. B., & Van Ness, J. W. (1968). Fractional Brownian motions, fractional noises and applications. *SIAM review*, 10(4), 422-437. <http://dx.doi.org/10.1137/1010093>
- [11] Tate, N. J. (1998). Estimating the fractal dimension of synthetic topographic surfaces. *Computers & Geosciences*, 24(4), 325-334. [http://dx.doi.org/10.1016/S0098-3004\(97\)00119-2](http://dx.doi.org/10.1016/S0098-3004(97)00119-2)
- [12] Juneja, A., Lathrop, D. P., Sreenivasan, K. R., & Stolovitzky, G. (1994). Synthetic turbulence. *Physical Review E*, 49(6), 5179. <http://dx.doi.org/10.1103/PhysRevE.49.5179>
- [13] Wendt, H., Roux, S. G., Jaffard, S., & Abry, P. (2009). Wavelet leaders and bootstrap for multifractal analysis of images. *Signal Processing*, 89(6), 1100-1114.
- [14] Plourde, S. M., Marin, Z., Smith, Z. R., Toner, B. C., Batchelder, K. A., & Khalil, A. (2016). Computational growth model of breast microcalcification clusters in simulated mammographic environments. *Computers in biology and medicine*, 76, 7-13.
- [15] Mehdi, M. Z., Ayed, N. G. B., Masmoudi, A. D., Sellami, D., & Abid, R. (2017). An efficient microcalcifications detection based on dual spatial/spectral processing. *Multimedia Tools and Applications*, 76(11), 13047-13065.
- [16] N. S. Arikids, S. Skiadopoulos, A. Karajaliou, "B-spline active rays segmentation of microcalcifications in mammography", *Medical Physics*, vol. 35, no. 11, pp. 5161-5171, Nov. 2008. <http://dx.doi.org/10.1118/1.2991286>.
- [17] Mohanalin, P. K. Kalra, N. Kumar, "Microcalcification segmentation using normalized tsallis entropy: an automatic q" calculation by exploiting type II fuzzy sets", *IETE Journal of Research*, vol. 25, no. 2, pp. 90-96, Feb. 2009. <http://dx.doi.org/10.4103/0377-2063.53240>
- [18] Papadopoulos, A., Fotiadis, D. I., & Costaridou, L. (2008). Improvement of microcalcification cluster detection in mammography utilizing image enhancement techniques. *Computers in biology and medicine*, 38(10), 1045-1055.

- [19] Duarte, M. A., Alvarenga, A. V., Azevedo, C. M., Calas, M. J. G., Infantosi, A. F., & Pereira, W. C. (2015). Evaluating geodesic active contours in microcalcifications segmentation on mammograms. *Computer Methods and Programs in Biomedicine*, 122(3), 304-315. <http://dx.doi.org/10.1016/j.cmpb.2015.08.016>
- [20] Dhahbi, S., Barhoumi, W., & Zagrouba, E. (2015). Breast cancer diagnosis in digitized mammograms using curvelet moments. *Computers in biology and medicine*, 64, 79-90.
- [21] Malar, E., Kandaswamy, A., Chakravarthy, D., & Dharan, A. G. (2012). A novel approach for detection and classification of mammographic microcalcifications using wavelet analysis and extreme learning machine. *Computers in biology and medicine*, 42(9), 898-905.
- [22] Alasadi, A. H. H., & Al-Saedi, A. K. H. (2017). A Method for Microcalcifications Detection in Breast Mammograms. *Journal of medical systems*, 41(4), 68.
- [23] Hamilton, E. K., Jeon, S., Ramirez Cobo, P., Lee, K. S., & Vidakovic, B. (2011, November). Diagnostic classification of digital mammograms by wavelet-based spectral tools: A comparative study In *Bioinformatics and Biomedicine (BIBM)*, 2011 IEEE International Conference on (pp. 384-389). IEEE.
- [24] Beheshti, S. M. A., Ahmadi Noubari, H., Fatemizadeh, E., & Khalili, M. (2014). An efficient fractal method for detection and diagnosis of breast masses in mammograms. *Journal of digital imaging*, 27(5), 661-669. <http://dx.doi.org/10.1007/s10278-013-9654-z>
- [25] Beheshti, S. M. A., Noubari, H. A., Fatemizadeh, E., & Khalili, M. (2015). Classification of abnormalities in mammograms by new asymmetric fractal features. *Biocybernetics and Biomedical Engineering*.
- [26] George, L. E., & Mohammed, E. Z. (2011, October). Cancer tissues recognition system using box counting method and artificial neural network. In *Soft Computing and Pattern Recognition (SoCPar)*, 2011 International Conference of (pp.5-9).IEEE. <http://dx.doi.org/10.1109/socpar.2011.6089105>
- [27] Stojić, T., Reljin, I., & Reljin, B. (2006). Adaptation of multifractal analysis to segmentation of microcalcifications in digital mammograms. *Physica A: Statistical Mechanics and its Applications*, 367, 494-508.
- [28] Sahli, I. S., Bettaieb, H. A., Ben Abdallah, A., Bhour, I., & Bedoui, M. H. (2015, November). Detection and segmentation of microcalcifications in digital mammograms using multifractal analysis. In *Image Processing Theory, Tools and Applications (IPTA)*, 2015 International Conference on (pp. 180-184). IEEE. <http://dx.doi.org/10.1109/ipta.2015.7367122>
- [29] Duarte, M. A., Alvarenga, A. V., Azevedo, C. M., Infantosi, A. F. C., & Pereira, W. C. A. (2011, March). Automatic microcalcifications segmentation procedure based on Otsu's method and morphological filters. In *Health Care Exchanges (PAHCE)*, 2011 Pan American (pp. 102-106). IEEE. <http://dx.doi.org/10.1109/pahce.2011.5871858>
- [30] Singh, B., & Kaur, M. (2017). An Approach for Enhancement of Microcalcifications in Mammograms. *Journal of Medical and Biological Engineering*, 1-13.
- [31] Ciecholewski, M. (2017). Microcalcification Segmentation from Mammograms: A Morphological Approach. *Journal of digital imaging*, 30(2), 172-184.
- [32] Duarte, M. D. A., Alvarenga, A. V., Azevedo, C. M., Calas, M. J. G., Infantosi, A. F. C., & Pereira, W. C. D. A. (2013). Segmenting mammographic microcalcifications using a semi-automatic procedure based on Otsu's method and morphological filters. *Revista Brasileira de Engenharia Biomédica*, 29(4), 377-388.
- [33] Tricot, C. (1999). *Courbes et dimension fractale*, Springer Science & Business Media.
- [34] Otsu, N. (1979). "AA threshold selection method from grey scale histogram." *IEEE Transactions on Systems Man and Cybernetics*.
- [35] Jaccard, P.: Étude comparative de la distribution orale dans une portion des alpes et des jura. *Bulletin de la Société Vaudoise des Sciences Naturelles* 37, 547-579 (1901).
- [36] Dice, L. R. (1945). Measures of the amount of ecologic association between species. *Ecology*, 26(3), 297-302.
- [37] Heine, John J., et al. "On the statistical nature of mammograms." *Medical physics* 26.11 (1999): 2254-2265.
- [38] Plourde, Shayne M., et al. "Computational growth model of breast microcalcification clusters in simulated mammographic environments." *Computers in biology and medicine* 76 (2016): 7-13.
- [39] Reed, I. S., Lee, P. C., & Truong, T. K. (1995). Spectral representation of fractional Brownian motion in n dimensions and its properties. *Information Theory, IEEE Transactions on*, 41(5), 1439-1451. <http://dx.doi.org/10.1109/18.412687>
- [40] Stein, M. L. (2002). Fast and exact simulation of fractional Brownian surfaces. *Journal of Computational and Graphical Statistics*, 11(3), 587-599. <http://dx.doi.org/10.1198/106186002466>
- [41] Kestener, P., et al. (2001). "Wavelet-based multifractal formalism to assist in diagnosis in digitized mammograms." *Image Anal. Stereol* 20(3): 169-174.
- [42] Suckling J, The MiniMIAS database, Mammographic Image Analysis Society MIAS. <http://peipa.essex.ac.uk/info/mias.html>
- [43] Bousson, V., Bergot, C., Sutter, B., Levitz, P., & Cortet, B. (2012). Scientific Committee of the Groupe de Recherche et d'Information sur les Ostéoporoses. Trabecular bone score (TBS): available knowledge, clinical relevance, and future prospects. *Osteoporos Int*, 23(5), 1489-1501.
- [44] M.M. De Santo M, F. Tortorella, M. Vento, Automated classification of clustered microcalcifications by a multiple expert system, *Pattern Recogn.* 36 (2003) 1467–1477.
- [45] J.C. Fu, S. Lee, S.T.C. Wong, J.Y. Yeh, A.H. Wang, H.K. Wu, Image segmentation feature selection and pattern classification for mammographic microcalcifications, *Comput. Med. Imag. Graph.* 29 (2005) 419–429.
- [46] Ayman A. Abu Baker, R. S. Qahwaji, Musbah J. Aqel, Mohammad H. Saleh, Mammogram image size reduction using 16-8 bit conversion technique, *Int. J. Biomed. Sci.* 1 (2) (2006) 1306-1216.
- [47] Classification de Le Gal des microcalcifications mammaires. Available online: http://www.aly-abbara.com/echographie/biometrie/scores/microcalcification_classification_le_gal.html (accessed on 16-11-2017).